



## Prediction of oral drug absorption in humans by theoretical passive absorption model<sup>☆</sup>

Kouki Obata\*, Kiyohiko Sugano<sup>1</sup>, Ryoichi Saitoh, Atsuko Higashida, Yoshiaki Nabuchi, Minoru Machida, Yosinori Aso

*Pre-clinical Research Department I, Chugai Pharmaceutical Co. Ltd., 1–135 Komakado, Gotemba, Shizuoka 412–8513, Japan*

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### Abstract

The purpose of the present study was to examine the oral drug absorption predictability of the theoretical passive absorption model (TPAM). As chemical descriptors of drugs, the octanol/buffer distribution coefficient at pH 6.0 ( $D_{ow}$ ), intrinsic octanol–water partition coefficient ( $P_{ow}$ ),  $pK_a$ , and molecular weight (MW) were calculated from the chemical structure. Total passive intestinal membrane permeation consists of transcellular, paracellular and unstirred water layer (UWL) permeation. Transcellular permeation was modeled based on the pH-partition hypothesis with correction for cationic species permeation, and the independent variables were  $D_{ow}$ ,  $P_{ow}$ , and  $pK_a$ . Paracellular permeation was modeled as a size-restricted diffusion within a negative electrostatic field-of-force, and the independent variables were MW and  $pK_a$ . UWL permeation was modeled as diffusion across a water layer, and the independent variable was MW. Cationic species permeation in the transcellular permeation model and the effect of a negative electric field-of-force in the paracellular permeation model were the extensions to the previous TPAM. The coefficients of the paracellular and UWL permeation models were taken from the literature. A data set of 258 compounds with observed values of Fa% (the fraction of a dose absorbed in humans) taken from the literature was employed to optimize four fitting coefficients in the transcellular permeation model. The TPAM predicted Fa%, with root mean square errors of 15–21% and a correlation coefficient (CC) of 0.78–0.88. In addition, the TPAM predicted the effective human intestinal membrane permeability with a CC of 0.67–0.77, as well as the contribution of paracellular permeation. The TPAM was found to predict oral absorption from the chemical structure of drugs with adequate predictability for usage in drug discovery. © 2005 Elsevier B.V. All rights reserved.

**Keywords:** Oral absorption; Lipophilicity;  $pK_a$ ; Octanol; In silico; Permeability

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\* Corresponding author. Tel.: +81 550 87 6707; fax: +81 550 87 5397.

*E-mail address:* [obatakuk@chugai-pharm.co.jp](mailto:obatakuk@chugai-pharm.co.jp) (K. Obata).

<sup>1</sup> Present address: Global Research & Development, Nagoya Laboratories, Pharmaceutical Sciences, Science and Technology, Pharmaceutical R&D, Pfizer Inc., 5-2 Taketoyo, Aichi 470-2393, Japan.

## 1. Introduction

In the recent drug discovery and development process, in silico prediction of absorption, metabolism, distribution, and excretion (ADME) is recognized as a key technique (van de Waterbeemd and Gifford, 2003). Among ADME properties, oral absorption has been most intensively investigated for in silico prediction. As an oral absorption parameter, the fraction of a dose absorbed in humans (Fa%), the effective intestinal membrane permeability in humans ( $P_{\text{eff}}$ ), Caco-2 permeability, etc., have been studied as targets for in silico prediction (Wessel et al., 1998; Winiwarter et al., 1998; Zhao et al., 2001; Yamashita et al., 2002). Oral absorption from a solid dosage is determined by the dissolution rate, the solubility, and the intestinal membrane permeability (Yu and Amidon, 1999). Intestinal membrane permeation consists of transcellular, paracellular, and unstirred water layer (UWL) permeation. Most of the previous in silico prediction studies scrambled these absorption processes, and the contribution of each process cannot be predicted. In addition, the previous in silico methods often used descriptors that are not easy to translate into better drug design.

Previously, the theoretical passive absorption model (TPAM) had been proposed for describing passive intestinal membrane permeation (Camenisch et al., 1996, 1998). The TPAM consists of three partial models, i.e., the transcellular, paracellular and UWL permeation models. The TPAM is beneficial for qualitatively comprehending the membrane permeation from the viewpoint of both the physiology of the intestine and the chemical structure of drugs. However, the predictability of the TPAM for the oral absorption in humans has not been examined. The purpose of the present study was to quantitatively examine the oral drug absorption predictability of the TPAM.

## 2. Calculation

### 2.1. Transcellular permeation model

Passive transcellular permeation is diffusion across a lipid bilayer. Therefore, the permeability depends on the lipophilicity of the permeant. In the previous TPAM, the passive transcellular permeability ( $P_{\text{trans}}$ ) was expressed by the 1-octanol/buffer distribution coefficient ( $D_{\text{ow}}$ ), with the help of so-called Collander

equations (Collander, 1950, 1951; Camenisch et al., 1998).

$$P_{\text{trans}} = a \cdot D_{\text{ow}}^{\alpha} \quad (1)$$

To reflect the pH at the intestinal epithelial membrane surface, the  $D_{\text{ow}}$  at pH 6.0 was employed (Maxwell et al., 1968). The pragmatic reason for using the 1-octanol/buffer system is its high publicity in the drug discovery process (Kerns and Di, 2003). Furthermore, various computational prediction systems have been developed for 1-octanol/buffer system (van de Waterbeemd and Gifford, 2003). Because the intrinsic octanol/water partition coefficient of ionized species is negligibly small, Eq. (1) represents the permeation of non-ionized species (pH-partition hypothesis) (Hogben et al., 1959). However, recently, the permeability of basic compounds was found to be larger than expected from the  $D_{\text{ow}}$  (Sugano et al., 2001). It was suggested that cationic species of basic compounds can permeate the negatively charged membrane with the aid of anionic lipids in the membrane, depending on the lipophilicity of the cationic species (Neubert et al., 1988; Ozaki et al., 2000; Sugano et al., 2001, 2004). The intestinal epithelial membrane contains anionic lipids (Proulx, 1991; Lipka et al., 1991). Therefore, Eq. (1) was extended for the permeability of mono-cationic species of basic compounds. The lipophilicity of the cationic species may be scaled by the octanol–water partition coefficient ( $P_{\text{ow}}$ ) of neutral species, with the help of Collander equations (Collander, 1950, 1951). Eq. (1) was extended to:

$$P_{\text{trans}} = a \cdot D_{\text{ow}}^{\alpha} + b \cdot f_{+1} \cdot P_{\text{ow}}^{\beta} \quad (2)$$

where  $f_{+1}$  is the fraction of mono-cationic species. The  $f_{+1}$  was calculated from the  $\text{p}K_{\text{a}}$ . Coefficients  $a$ ,  $b$ ,  $\alpha$ , and  $\beta$  are fitting parameters to be optimized in the present study.

### 2.2. Paracellular permeation model

Paracellular permeation is diffusion through the negatively charged tight junction between the intestinal epithelial cells, and was modeled by a size-restricted diffusion within a negative electrostatic field-of-force (Adson et al., 1994, 1995; Sugano et al., 2002, 2003). Small and cationic species can easily permeate the paracellular pathway, whereas large and anionic

species permeates little. As a molecular-sieving function, the Renkin function ( $F(B)$ , Eq. (4)) was employed. In addition, an electric field-of-force function ( $E(Z)$ , Eq. (6)) was employed, as an extension to the previous TPAM (Camenisch et al., 1996, 1998). The paracellular permeability ( $P_{\text{para}}$ ) is expressed as:

$$P_{\text{para}} = A \cdot \frac{1}{\text{MW}^{1/3}} \cdot F(B) \left( f_0 + \sum_{z(z \neq 0)} f_z \cdot E(z) \right) \quad (3)$$

$$F(B) = (1 - B)^2 (1 - 2.104 \cdot B + 2.09 \cdot B^3 - 0.95 \cdot B^5) \quad (4)$$

$$B = \frac{\text{MW}^{1/3}}{R_{\text{MW}}} \quad (5)$$

$$E(Z) = \frac{C \cdot z}{1 - e^{-C \cdot z}} \quad (6)$$

where  $z$  is the molecular charge,  $f_z$  the fraction of each charged species,  $\text{MW}$  the molecular weight, and  $R_{\text{MW}}$  is the apparent pore size of the paracellular pathway based on a  $\text{MW}$  scale. Previously, molecular volume was employed as a parameter of molecular size. However, in the present study,  $\text{MW}$  was employed, because  $\text{MW}$  is more public in the drug discovery process, and easier to calculate. The replacement of molecular volume to  $\text{MW}$  did not affect the predictability of the  $P_{\text{para}}$  model (data not shown).  $R_{\text{MW}}$ ,  $A$ , and  $C$  were previously optimized utilizing  $\text{Fa}\%$  and artificial membrane permeability data, as previously reported (Sugano et al., 2002).  $R_{\text{MW}} = 8.46$ ,  $A = 2.41 \times 10^{-2}$ , and  $C = 2.39$  were used in the present study.

### 2.3. Unstirred water layer permeation model

The UWL is adjacent to the intestinal epithelial membrane. UWL permeation was modeled as a simple diffusion process in a water layer. The UWL permeability ( $P_{\text{UWL}}$ ) is reciprocal to  $\text{MW}^{1/3}$  (Larhed et al., 1997). Previously, the  $P_{\text{eff}}$  of glucose, the permeation of which is rate-limited by the UWL, was reported to be  $10 \times 10^{-4}$  cm/s (Lennernäs, 1998).  $\text{MW}$  of glucose is 180. Therefore, the  $P_{\text{UWL}}$  of each drug is expressed as:

$$P_{\text{UWL}} = 10 \times 10^{-4} \left( \frac{180}{\text{MW}} \right)^{1/3} \quad (7)$$

### 2.4. Total passive intestinal membrane permeability and $\text{Fa}\%$

It may be assumed that total resistance to permeation ( $R_{\text{tot}}$ ) is the sum of the resistances of the membrane ( $R_{\text{m}}$ ) and UWL ( $R_{\text{UWL}}$ ) on the membrane:

$$R_{\text{tot}} = R_{\text{m}} + R_{\text{UWL}} \quad (8)$$

Resistance is the inverse of permeability. Therefore, the total passive permeability across the intestinal membrane ( $P_{\text{tot}}$ ) is expressed by the membrane permeability ( $P_{\text{m}}$ ) and  $P_{\text{UWL}}$  (Camenisch et al., 1996; Pade and Stavchansky, 1997).

$$\frac{1}{P_{\text{tot}}} = \frac{1}{P_{\text{m}}} + \frac{1}{P_{\text{UWL}}} \quad (9)$$

$P_{\text{m}}$  is the sum of  $P_{\text{trans}}$  and  $P_{\text{para}}$ . Therefore,  $P_{\text{tot}}$  is converted to:

$$\frac{1}{P_{\text{tot}}} = \frac{1}{P_{\text{trans}} + P_{\text{para}}} + \frac{1}{P_{\text{UWL}}} \quad (10)$$

The contributions of the transcellular pathway permeability of neutral species ( $\text{Trans}_n\%$ ), mono-cationic species ( $\text{Trans}_c\%$ ), and the paracellular pathway permeability ( $\text{Para}\%$ ) to  $P_{\text{m}}$  are expressed as:

$$\text{Trans}_n\% = \frac{a \cdot D_{\text{ow}}^\alpha}{P_{\text{m}}} \times 100 \quad (11)$$

$$\text{Trans}_c\% = \frac{b \cdot f_{+1} \cdot P_{\text{ow}}^\beta}{P_{\text{m}}} \times 100 \quad (12)$$

$$\text{Para}\% = \frac{P_{\text{para}}}{P_{\text{m}}} \times 100 \quad (13)$$

The contribution of the UWL to the total resistance is expressed as:

$$R_{\text{UWL}}\% = \frac{R_{\text{UWL}}}{R_{\text{tot}}} \times 100 = \left( 1 - \frac{P_{\text{tot}}}{P_{\text{m}}} \right) \times 100 \quad (14)$$

When we employ a plug-flow model as an absorption model from the intestinal tube (Yu and Amidon, 1999), the calculated  $\text{Fa}\%$  is expressed as:

$$\text{Fa}\%_{\text{calc}} = (1 - \exp(-Gz \cdot P_{\text{tot}})) \times 100 \quad (15)$$

where  $Gz$  is the lump constant of available intestinal surface area and transit time. In the present study,  $Gz = 1.39 \times 10^4$  was employed to arrange the

scale identical between  $P_{\text{tot}}$  and  $P_{\text{eff}}$  (cm/s) (Yu and Amidon, 1999).

### 2.5. Human intestinal absorption data and physicochemical parameters

Three hundred forty three observed Fa% values ( $\text{Fa\%}_{\text{obs}}$ ) were collected from literature compilations, and stored in the in-house database (Noel, 1979; Dressman et al., 1985; Taylor et al., 1985; Artursson and Karlsson, 1991; Chong et al., 1996; Walter et al., 1996; Palm et al., 1997; Yee, 1997; Chiou and Barve, 1998; Chiou et al., 2000; McEvoy, 1998; Yazdaniyan et al., 1998; Balon et al., 1999; Irvine et al., 1999; Wessel et al., 1998; Winiwarter et al., 1998; Karlsson et al., 1999; Wohnsland and Faller, 2001; Zhao et al., 2001). Most of these literatures were in silico–in vitro correlation or in vitro–in vivo correlation studies. Therefore, we assumed that Fa% data from these literatures compilations were also suitable for the purpose of the present study. In addition, drugs which undergo active transport (both influx and efflux), intestinal metabolism, and solubility-limited absorption were excluded from the analysis (Adair and McElnay, 1987; Adam and Timmler, 1982; Avdeef, 2001; Behrens et al., 2001; Chiou et al., 2001; Chong et al., 1996; Dantzig et al., 1992; Eneroth et al., 2001; Fraga Fuentes et al., 1997; Groen et al., 1988; Hashida, 1995; Hochman et al., 2001; Holdiness, 1984; Kim et al., 1998; Koup et al., 1988; Liang et al., 2000; Matsuda et al., 1998a,b; McEvoy, 1998; Nicolaos et al., 2003; Orłowski et al., 1998; Overdiek and Merkus, 1986; Poschet et al., 1996; Pradhan and Majumdar, 1986; Schanker et al., 1963; Seelig, 1998; Shu et al., 2001; Smith et al., 2001; Takanaga et al., 1994; Tamai and Tsuji, 1996; Thwaites et al., 1994; Tsuji et al., 1982; Wakasugi et al., 1998; Walter et al., 1996; Welker et al., 1998; Wenzel et al., 1996; Williams and Harding, 1984; Yee, 1997). Drugs with  $\log D_{\text{ow}} > 4$  were excluded because low solubility was expected (Yalkowsky and Valvani, 1980; Avdeef, 2003). Quaternary ammonium compounds and polymers were also excluded because Pallas 3.1 (CompuDrug, Hungary) could not calculate  $\log P_{\text{ow}}$  adequately.

Typical  $\text{Fa\%}_{\text{obs}}$  values and physicochemical parameters are shown in Table 1. The  $D_{\text{ow}}$  at pH 6.0,  $P_{\text{ow}}$  and  $\text{p}K_{\text{a}}$  were calculated from the chemical structure of drugs by Pallas 3.1. When the drug contained

ortho-carbonyl phenol fragment, 0.55 per fragment was added to  $\log P_{\text{ow}}$  and  $\log D_{\text{ow}}$  (Pallas was found to underestimate these drug's  $\log P_{\text{ow}}$  at an average of 0.55 (data not shown)).

### 2.6. Optimization of coefficients

Coefficients  $a$ ,  $b$ ,  $\alpha$ , and  $\beta$  in the transcellular permeation model (Eq. (2)) were optimized by fitting Eq. (15) to  $\text{Fa\%}_{\text{obs}}$  values using the least square method. Eqs. (2)–(7) were converted to  $P_{\text{tot}}$  by inserting into Eq. (10), and Eq. (10) was converted to Fa% by inserting into Eq. (15). The sum of squares of the difference between  $\text{Fa\%}_{\text{calc}}$  and  $\text{Fa\%}_{\text{obs}}$  ( $\text{Fa\%}_{\text{diff}}$ ) was minimized using the Quasi-Newton method (EXCEL 2000, Microsoft, Redmont, WA). After preliminary optimization of the prediction scheme, large outliers are additionally surveyed by literature and excluded if they were reported to undergo active transport, intestinal metabolism, and solubility-limited absorption.

## 3. Results and discussion

Previously, Wenlock et al. (2003) reported that the mean  $\log D_{\text{ow}}$  (pH 7.4) of the marketed oral drugs was 1.0 and the standard deviation was 3.4. Distribution of  $\log D_{\text{ow}}$  (pH 7.4) and electrical charge of drugs collected in this study ( $N=343$ ) is shown in Fig. 1. The mean  $\log D_{\text{ow}}$  (pH 7.4) was  $-0.41$  and the standard deviation was 3.3. After excluding efflux substrates, intestinal metabolism substrates and low solubility drugs, the mean  $\log D_{\text{ow}}$  (pH 7.4) was  $-0.62$  and the

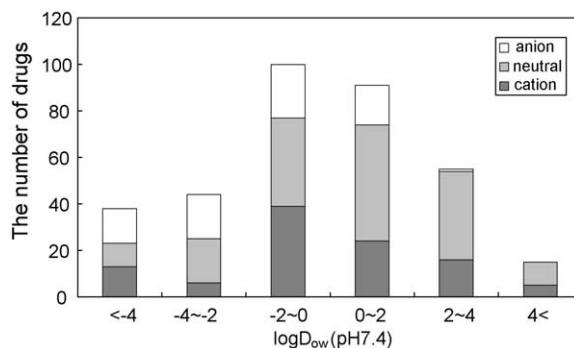


Fig. 1. Distribution of calculated  $\log D_{\text{ow}}$  (pH 7.4) and electrical charge of drugs used in this study.

Table 1  
Fa%, physicochemical properties, and predicted oral absorption parameters

No.	Compound	MW	pK <sub>a</sub> <sup>a,b</sup>	log P <sub>ow</sub> <sup>a</sup>	log D <sub>ow</sub> <sup>a</sup>	Fa% <sub>obs</sub> <sup>c</sup>	log P <sub>eff</sub> <sup>c</sup>	Fa% <sub>calc</sub> <sup>e</sup>	log P <sub>tot</sub> <sup>e</sup>	Trans <sub>n</sub> % <sup>e</sup>	Trans <sub>c</sub> % <sup>e</sup>	Para% <sup>e</sup>	R <sub>UWL</sub> % <sup>e</sup>
1	Amiloride	230	5.26 (b)	-1.03	-1.10	50	-3.79	70	-4.06	65	3	32	9
2	Antipyrine	188		1.79	1.79	97	-3.35	100	-3.26	97	0	3	55
3	Atenolol	266	10.08 (b)	0.44	-2.10	50	-4.70	72	-4.04	22	34	44	10
4	Carbamazepine	236		2.28	2.28	<sup>d</sup>	-3.37	100	-3.20	99	0	1	68
5	Cimetidine	241	6.71 (b)	-0.09	-0.87	64	-4.52	84	-3.88	51	16	33	15
6	Creatinine	113		-1.82	-1.82	80	-4.52	84	-3.88	20	0	80	11
7	Desipramine	266	10.63 (b)	4.00	0.67	100	-3.36	99	-3.48	70	22	8	38
8	Fluvastatine	411	4.32 (a)	4.71	3.03	100	-3.62	100	-3.19	100	0	0	85
9	Furosemide	331	4.06 (a)	2.20	0.25	61	-5.30	93	-3.72	99	0	1	23
10	Hydrochlorothiazide	298		-0.36	-0.36	67	-5.40	82	-3.91	92	0	8	14
11	Ketoprofen	254	3.49 (a)	3.67	1.18	100	-3.08	99	-3.43	99	0	1	42
12	Metoprolol	267	10.08 (b)	1.97	-0.90	95	-3.89	87	-3.83	43	33	24	17
13	Naproxen	230	4.06 (a)	3.26	1.32	99	-3.08	100	-3.39	99	0	1	44
14	Piroxicam	331	4.66 (b)	0.45	0.43	100	-3.11	95	-3.65	96	1	3	27
15	Propranolol	259	10.08 (b)	3.00	-0.08	90	-3.54	96	-3.64	57	27	15	26
16	Ranitidine	314	9.04 (b)	0.79	-1.71	50	-4.57	71	-4.05	34	39	27	11
17	Terbutaline	225	12.01 (b)	1.07	-1.63	62	-4.52	83	-3.90	25	29	46	14
18	Acyclovir	225		-2.08	-2.09	20	<sup>d</sup>	47	-4.34	47	0	53	5
19	Ceftriaxone	555	2.33 (a)	-1.53	-4.68	1	<sup>d</sup>	2	-5.79	98	0	2	0
20	Cefuroxime	424	2.12 (a), 6.10 (b)	-1.09	-3.29	5	<sup>d</sup>	11	-5.08	78	0	22	1
21	Oxacillin	401	2.52 (a)	1.56	-1.69	33	<sup>d</sup>	37	-4.48	97	0	3	4
22	Timolol	316	10.5 (b)	0.51	-2.06	90	<sup>d</sup>	66	-4.11	27	42	31	9

<sup>a</sup> Calculated by Pallas 3.1.

<sup>b</sup> The pK<sub>a</sub> values of the acid (pK<sub>a</sub> < 7.3) and base (pK<sub>a</sub> > 4.6) are indicated ((a): acid and (b): base).

<sup>c</sup> Obtained from the literature listed in the text.

<sup>d</sup> Not reported.

<sup>e</sup> Calculated with the coefficients set V in Table 2.

Table 2  
Fitting coefficients and Fa% predictability statistics

Set	<i>N</i>	<i>a</i> ( $\times 10^{-4}$ )	$\alpha$	<i>b</i> ( $\times 10^{-4}$ )	$\beta$	RMSE	CC
I	258	1.4	0.32	0.23	0.19	19	0.81
II <sup>a</sup>	258	1.3	0.34	0.43	0.14	19	0.80
III <sup>b</sup>	258	1.6	0.29			20	0.80
IV <sup>a,b</sup>	258	1.8	0.29			21	0.78
V	242	1.9	0.44	0.30	0.15	15	0.88
VI <sup>a</sup>	242	1.8	0.46	0.50	0.13	16	0.87
VII <sup>b</sup>	242	2.1	0.38			16	0.87
VIII <sup>a,b</sup>	242	2.3	0.35			18	0.84

<sup>a</sup> Without the extension for electric field-of-force in paracellular pathway model.

<sup>b</sup> Without the extension for cationic species permeation in transcellular pathway model.

standard deviation was 2.8 ( $N = 258$ ). The drugs used in this study were biased to low lipophilicity, comparing with the marketed oral drugs. Because  $\log D_{ow}$  of dissociable molecule is lower than that of neutral species, the percentage of neutral compounds would increase at high  $\log D_{ow}$ .

Coefficients *a*, *b*,  $\alpha$ , and  $\beta$  were optimized using 258 Fa%<sub>obs</sub> values (Table 2, the coefficients set I–IV). Sixteen large outliers (Fa%<sub>diff</sub> > 2 × root mean square error (RSME)) were identified. Eight of these outliers were due to the p*K*<sub>a</sub> and *P*<sub>ow</sub> calculation error (data not shown). Other outliers were amphotericin B (Fa%<sub>obs</sub>, Fa%<sub>calc</sub>: 5%, 44% (same order in the following parentheses)), carfecillin (100%, 59%), cymarlin (47%, 97%), dantrolene (35%, 98%), mercaptethane-sulfonic acid (77%, 27%), metaproterenol (44%, 83%), miglitol (100%, 59%), and nizatidine (100%, 61%). Reasons for these outliers could not be clarified by a literature survey. Optimization of *a*, *b*,  $\alpha$ , and  $\beta$  without large outliers was also performed (Table 2, the coefficients set V–VIII).

The relationship between Fa%<sub>obs</sub> and Fa%<sub>calc</sub> with the coefficients set V is shown in Fig. 2A. In addition, the relationship between Fa%<sub>obs</sub> and *P*<sub>tot</sub> is shown in Fig. 2B. Correlation coefficients (CC) and RMSE, which are predictability indicators, are summarized in Table 2. The TPAM calculated Fa% with adequate correlation (CC = 0.78–0.88, RMSE = 15–21). Therefore, the TPAM was suggested to be applicable for drug discovery. Without the extensions to the previous TPAM, i.e., the negative electric field-of-force in the paracellular permeation model and the cationic species permeation in the transcellular permeation model, predictability was slightly lowered (Table 2).

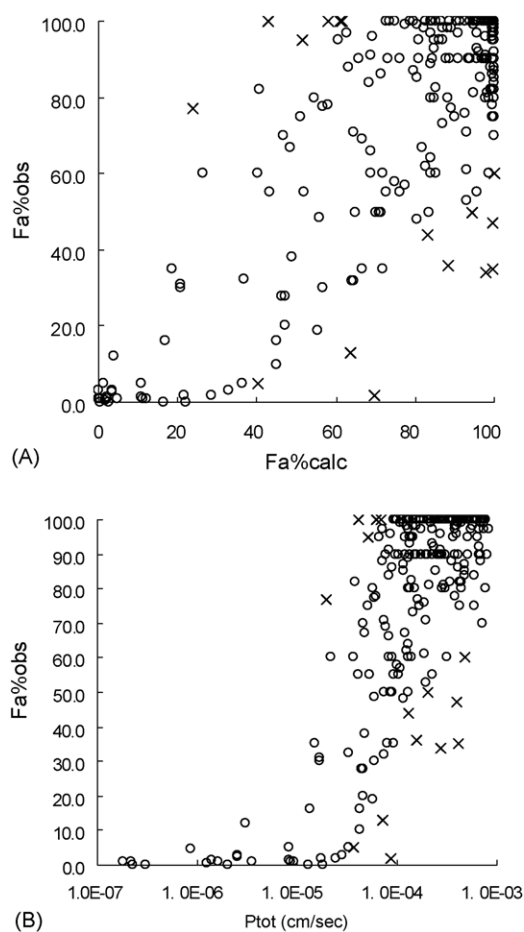


Fig. 2. Relationship between calculated oral absorption data and observed Fa%. (A) Fa%<sub>obs</sub> vs. Fa%<sub>calc</sub>. (B) Fa%<sub>obs</sub> vs. *P*<sub>tot</sub>. Fa%<sub>calc</sub> and *P*<sub>tot</sub> were calculated with the coefficients set V in Table 2. Cross indicates large outliers excluded from the analysis (see text).

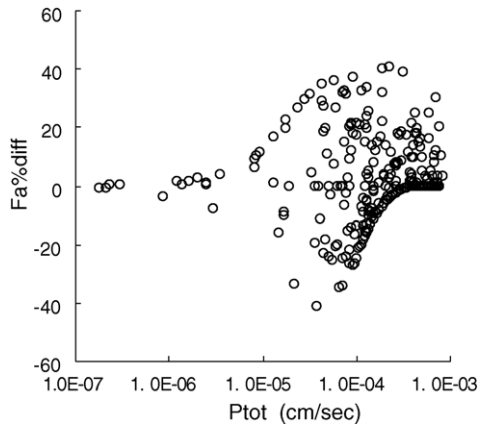


Fig. 3. Relationship between  $P_{\text{tot}}$  and  $\text{Fa}\%_{\text{diff}}$ .  $\text{Fa}\%_{\text{diff}}$  was calculated with the coefficients set V in Table 2.

The relationship between  $P_{\text{tot}}$  and  $\text{Fa}\%_{\text{diff}}$  with coefficients set V is shown in Fig. 3. The  $\text{Fa}\%_{\text{diff}}$  was largest around  $\log P_{\text{tot}} = -4.5$ , probably because the  $\text{Fa}\% - \log P_{\text{tot}}$  relationship was sigmoidal, and had a large slope around this  $\log P_{\text{tot}}$  value (Fig. 2B). From Fig. 3, we can estimate the prediction probability. Prediction probability is important information for decision-making in drug discovery, however it was not often considered in the previous in silico studies.

The relationship between  $P_{\text{eff}}$  and  $P_{\text{tot}}$  with coefficients set V was also investigated (Fig. 4).  $P_{\text{eff}}$  values were measured using a technique based on single-pass perfusion of a human jejunum segment between two inflated balloons (Lennernäs, 1998). Eighteen in vivo  $P_{\text{eff}}$  values were collected from the literature (Winiwarter

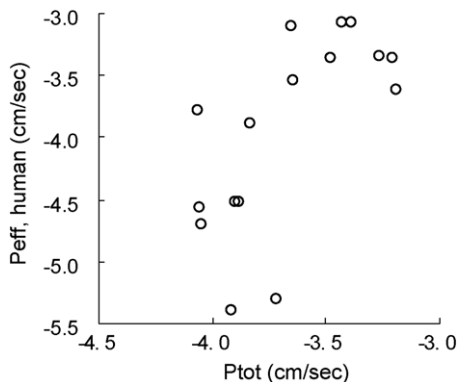


Fig. 4. Relationship between  $P_{\text{tot}}$  and  $P_{\text{eff}}$ .  $P_{\text{tot}}$  was calculated with the coefficients set V in Table 2.

et al., 1998; Takamatsu et al., 2001; Lennernäs et al., 2002).  $P_{\text{eff}}$  of actively transported compounds were excluded.  $P_{\text{tot}}$  correlated to  $P_{\text{eff}}$  with  $\text{CC} = 0.67$  (set V).  $P_{\text{eff}}$  of furosemide and hydrochlorothiazide were underestimated. However, their  $P_{\text{eff}}$  were also lower than expected from their  $\text{Fa}\%$  (61% and 67%) and Caco-2 permeability ( $0.11 \pm 0.01$  and  $0.42 \pm 0.03$  ( $\times 10^{-6}$  cm/s)) (Wessel et al., 1998; Yamashita et al., 2000), suggesting that their  $P_{\text{eff}}$  could have been under assessed. Without furosemide and hydrochlorothiazide,  $P_{\text{tot}}$  correlated to  $P_{\text{eff}}$  with  $\text{CC} = 0.77$ .

Relative contributions of paracellular permeation ( $\text{Para}\%$ ) and transcellular permeation ( $\text{Trans}_n\%$  and  $\text{Trans}_c\%$ ) were calculated with coefficients set V (Table 1). Previously, in Caco-2 at pH 5.4, the relative contributions of paracellular permeation for cimetidine, furosemide, naproxen, and propranolol were reported to be 31%, 1%, 0%, and 3%, respectively (Pade and Stavchansky, 1997). In the present study, they were predicted as 33%, 1%, 1%, and 15%, respectively. Therefore, it is suggested that the TPAM adequately predicted the main permeation pathway. Relative contribution of mono cationic species permeation ( $\text{Trans}_c\%$ ) in metoprolol and timolol were 33% and 42%, respectively (Table 1). Previously, the permeability of basic compounds across bio-mimetic artificial membrane was found to be larger than expected from the  $D_{\text{ow}}$ , suggesting that contribution of the permeation of cationic species is significant (Sugano et al., 2001, 2004). Relative contribution of the UWL to the total resistance was also calculated (Table 1). The UWL of the gastrointestinal tract was maintained by mucus layer. In case of fluvastatine, because of its high lipophilicity ( $\log D_{\text{ow}} = 3.03$ ), the transcellular pathway permeability could be high ( $\log P_{\text{trans}} = -2.38$ ). However, the UWL resistance was suggested to be more effective on total resistance to permeation ( $R_{\text{UWL}}\% = 85\%$ ) than the membrane resistance. Consequently, the total permeability could be settled in the upper limit ( $\log P_{\text{tot}} = -3.19$ ,  $\log P_{\text{eff}} = -3.62$ ).

Prediction of the permeation mechanism, which was not incorporated in the previously reported in silico methods, is an advantage of the TPAM approach. Permeation mechanism is important information for rational drug design. In addition, the TPAM approach has several other pragmatic advantages. The prediction scheme is explicit and corresponds to physiological structure of intestinal membrane. In the present TPAM

study, simple molecular descriptors, which are public and available to most drug discovery scientists were utilized. The possibility of over-learning is low, because only four fitting coefficients in the transcellular permeation model were optimized by fitting with hundreds of  $Fa\%_{obs}$  values. The coefficients in the paracellular and UWL permeation models had been derived and checked by physiological and/or model experiments. These features of TPAM may increase the accountability for users in the drug discovery stage.

In conclusion, for the use in drug discovery, the TPAM has adequate predictability and provides information about permeation pathway for drug discovery scientists. To improve the predictability, the effect of villosity of the intestinal membrane and pH variation along the absorption process can be incorporated to the TPAM (Said et al., 1986; Winne, 1989). Also, additional molecular descriptors might be required for the transcellular permeation model to correct the difference between octanol and the phospholipid bilayer (Zhao et al., 2001). The parallel artificial membrane permeability assay, which is an assay for passive transcellular permeation, may contribute to increasing the predictability of the transcellular permeation model (Kansy et al., 1998; Sugano et al., 2001; Avdeef, 2003). To predict the oral absorption of low solubility compounds, solubility/dissolution processes and the gastro-intestinal transit process are additionally required (Yu and Amidon, 1999). In addition, effects of transporters and intestinal metabolisms can be incorporated to the TPAM. These further extensions to the TPAM may complicate the prediction scheme. However, the prediction scheme may still possess divisibility and provide mechanistic insights. Therefore, the advantages of the TPAM approach may not be compromised by these extensions.

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